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Monitoring of β -Amyloid Dynamics after Human Traumatic Brain Injury

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Abstract

Epidemiological evidence links severe or repeated traumatic brain injury (TBI) to the development of Alzheimer's disease (AD). Accumulation of amyloid precursor protein (APP) occurs with high frequency after TBI, particularly in injured axons, and APP may be cleaved to amyloid- β ($A\beta$) peptides playing key pathophysiological roles in AD. We used cerebral microdialysis (MD) to test the hypothesis that interstitial $A\beta$ levels are altered following TBI and are related to the injury type, cerebral energy metabolism, age of the patient, and level of consciousness. In the present report, we evaluated 10 mechanically ventilated patients (7 male, 3 female, ages 18–76 years) with a severe TBI, who had intracranial pressure and MD monitoring. Each MD sample was analyzed for hourly routine energy metabolic biomarkers (MD-lactate, MD-pyruvate, MD-glucose, and MD-lactate/pyruvate ratio), cellular distress biomarkers (MD-glutamate, MD-glycerol), and MD-urea. The remaining MD samples were analyzed for $A\beta$ 1–40 ($A\beta$ 40; $n=765$ samples) and $A\beta$ 1–42 ($A\beta$ 42; $n=765$ samples) in pooled 2 h fractions up to 14 days post-injury, using the Luminex xMAP technique, allowing detection with high temporal resolution of the key $A\beta$ peptides $A\beta$ 40 and $A\beta$ 42. Data are presented using medians and 25th and 75th percentiles. Both $A\beta$ 40 and $A\beta$ 42 were consistently higher in patients with predominately diffuse axonal injury compared with patients with focal TBI at days 1–6 post-injury, $A\beta$ 42 being significantly increased at 113–116 h post-injury ($p<0.05$). The $A\beta$ levels did not correlate with the interstitial energy metabolic situation, age of the patient, or the level of consciousness. These results support that interstitial generation of potentially toxic $A\beta$ species may occur following human TBI, particularly related to axonal injury.

Key words: $A\beta$; APP; axonal injury; cerebral MD; energy metabolism; TBI

Introduction

TRAUMATIC BRAIN INJURY (TBI) frequently causes long-term sequelae such as cognitive impairment, personality changes, and depression leading to social problems and a reduced quality of life.^{1,2} The chronic disabilities associated with apparently mild TBI, occurring from some blast injuries sustained in the military setting or during sport activities, are also increasingly recognized.^{3,4} Epidemiological evidence links severe or repeated TBI to the development of Alzheimer's disease (AD).^{5–10} Amyloid- β ($A\beta$) plaques, a hallmark pathological finding observed in the brains of AD patients, have been observed in a subset of TBI patients within hours post-injury.^{5,11,12} The membrane glycoprotein amyloid precursor protein (APP) is synthesized in the neuronal cytoplasm, and accumulates within injured axons following

TBI.^{5,13–16} APP may be proteolytically cleaved by different enzymes including α -secretase, preventing the generation of $A\beta$ peptides, or the β -site APP cleaving enzyme 1 (BACE1). BACE1-mediated APP cleavage, combined with γ -secretase-mediated cleavage of the remaining APP stub, leads to the generation of amyloid- β ($A\beta$) peptides of various lengths, including the 40 and 42 amino acid long $A\beta$ peptides.^{17–20} BACE1 and presenilin, important for $A\beta$ generation, have also been found to accumulate in injured and swollen axons post-injury.^{21,22} Although normal neuronal activity can produce $A\beta$ via APP processing,²³ these findings make the formation of $A\beta$ peptides a likely consequence of axonal injury. Importantly, inhibition of APP β - or γ -secretases improves outcome in experimental TBI.²⁴ As β - and γ -secretase-generated $A\beta$ forms are released into the interstitial fluid, cerebral microdialysis (MD) is a preferred sampling method for these biomarkers.^{25,26}

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One predominant goal of neurocritical care (NCC) is the detection and avoidance of cerebral ischemia. Ischemic brain damage has long been considered a major secondary injury mechanism in TBI.²⁷ In modern NCC, MD may be used to detect patterns suggestive of ischemia such as an elevated MD lactate/pyruvate ratio (LPR)^{28–30} combined with a reduced interstitial glucose (MD-glc^{31,32}). In a recent study on 223 TBI patients, MD-LPR and MD-glc were found to be independent predictors of poor outcome.³³ Experimental cerebral ischemia leads to increased APP production and upregulation of BACE activity.^{34–36} Additionally, cerebral ischemia has been associated with increased production of Aβ from APP, both in experimental models^{37,38} and in humans.^{39–41} These reports suggest a link between energy metabolic disturbance and Aβ peptide formation.

Experimentally, Aβ may also have direct neurotoxic properties,^{42–44} and, therefore, be important for the pathophysiology of TBI. In three recent publications,^{25,26,45} MD was used to detect interstitial Aβ formation early following severe TBI in humans. Using an Aβ(1-x) enzyme-linked immunosorbent assay (ELISA) not directly measuring Aβ40 or Aβ42, MD- Aβ levels were found to correlate with the level of consciousness in neurovascular and TBI patients in an NCC setting.²⁶ In another report, the temporal patterns of Aβ peptides could be studied in 12 h fractions using a sandwich ELISA.²⁵ The results of this pilot study showed that Aβ42 was consistently higher in patients with diffuse TBI, calling for additional studies of this potentially useful biomarker of diffuse axonal injury (DAI). However, the sensitivity of the assay was limited. In the present report, we used the Luminex technique to improve the analytical sensitivity to enhance the temporal resolution of Aβ peptide dynamics in 10 patients with moderate to severe TBI. Our main hypotheses were that Aβ peptide levels would correlate with the presence of diffuse brain injury, indicating axonal injury, cerebral energy metabolic perturbation, patient age, and the level of consciousness.

Methods

All research procedures described herein were approved by the Regional Research Ethics Committee at Uppsala University and informed consent was obtained from the patient’s closest relative.

This single center study was performed in a university hospital NCC setting.

Patient population and neurocritical care management

We included 10 patients (7 male, 3 female) conveniently recruited with a severe TBI, defined as a post-resuscitation Glasgow Coma Scale (GCS) score ≤ 8 at the primary hospital. On arrival in our unit, all patients were intubated and the motor component of the GCS (the Glasgow Motor Scale [GMS]) is presented in Table 1. No patient had a previous history of a neurodegenerative disease or Down’s syndrome. All patients required treatment in a NCC setting, including intubation and mechanical ventilation, and were managed according to a standardized brain injury protocol aiming to keep intracranial pressure (ICP) at ≤ 20 and cerebral perfusion pressure (CPP) at ≥ 60 mm Hg.^{46,47} ICP was monitored in all patients, either with an intraparenchymal ICP monitor (Codman, Johnson & Johnson, six patients), an external ventricular drain (three patients) or both (one patient). We used a sedation protocol in which patients were sedated using continuous intravenous propofol infusion (1–4 mg/kg/h Propofol-Lipuro; B. Braun Melsungen AG, Melsungen, Germany) combined with intermittent intravenous morphine (1–3 mg Morfin Meda; Meda, Sollentuna, Sweden). When ICP elevations could not be controlled using standard therapy, continuous sodium pentobarbital infusion therapy was initiated in one patient. Volume substitution and/or inotropic agents (Dobutamine or norepinephrine) were administered when needed. Plasma glucose was frequently evaluated and maintained at 5–10 mmol/L where insulin was administered when plasma glucose levels reached > 10 mmol/L. A neurological examination was performed regularly, up to six times daily, using the neurological wake-up test to register the motor component of the GCS (the GMS) and focal neurological signs on computerized observation charts.⁴⁶ For presentation of data, the patients were classified into conscious (GMS = 6) or not (GMS < 6) during the time for Aβ sampling (described subsequently). Additional injuries were scored according to the New Injury Severity Score (NISS), ranging from 1 to 75.⁴⁸ At ~ 6 months post-injury, patient outcome was assessed using the extended Glasgow Outcome Scale (eGOS⁴⁹).

Radiological analysis

CT scans were frequently performed as part of the monitoring strategy. When analyzing each CT scan, the “worst” CT scan (i.e.,

TABLE 1. CLINICAL CHARACTERISTICS OF EACH PATIENT INCLUDED IN THIS STUDY

Case no.	Group	Age (yrs), sex	Cause of injury	NISS/associated conditions ^a	GMS scores on arrival	Pupils	MD duration (h) ^c	LOS/ extubation (days)	GMS score on departure	eGOS
1	Focal/mixed	76, M	Fall	51	6	Normal	8–214	21/8	6	4
2	DAI	42, M	MVA	50	2	Bilat small	17–346	17/7	3	3
3	DAI	52, F	MVA	^a	3	Rt dilated	19–145	8/6	6	4
4	Focal/mixed	19, M	MVA	57	5	Normal	24–150	18/14	6	8
5	DAI	25, F	MVA	38	5	Normal	14–164	7/6	6	8
6	Focal/mixed	31, M	MVA	29	3	Rt dilated	7–147	10/9	5	5
7	Focal/mixed	43, M	Tire explosion	30	4	Normal	13–58	6/2	6	7
8	DAI	35, F	Fall	19	5	Rt dilated	7–188	11/8	6	3
9	Focal/mixed	55, M	Fall	21 ^a	3	Bilat dilated unresponsive	13–273	20/17	4	4
10	DAI	18, M	MVA	29	4	Rt dilated	75–311	17/9	4	5

^aIsolated brain injury, NISS cannot be applied.

^bAlcohol indicates a high serum ethanol on arrival in the primary hospital.

^cNumber of hours post-injury at which the microdialysis was initiated and stopped; the interval between the numbers represents the total duration of microdialysis.

DAI, diffuse axonal injury; eGOS, extended Glasgow Outcome Scale at 6 months post-injury; GMS, motor component of the Glasgow Coma Scale; NISS, New Injury Severity Score; LOS, length of stay; MD, microdialysis; MVA, motor vehicle accident.

the CT scan with the most intracranial lesions and/or mass effect during the course of the disease) was selected and analyzed for each of the 10 patients.⁵⁰ We used the Marshall classification⁵¹ and divided the patients into having either a DAI or a focal/mixed TBI.²⁵ Radiological characteristics of focal/mixed TBI included focal lesions such as epi- and subdural hemorrhages and lobar contusions. Criteria for DAI were diffuse brain swelling and/or small petechial hemorrhages located at the gray/white matter junction, corpus callosum, and/or brainstem. Compression of basal cisterns was determined by the following scoring system: 0 = normal, 1 = compressed yet visible, 2 = compressed. The midline shift was calculated at the level of the thalami. The volume in milliliters of each mass lesion was calculated using the formula length × width × height/2.

MD procedure

The MD probe was inserted in conjunction with implantation of the ICP monitoring device, typically in the nondominant frontal lobe 1–2 cm anterior to the coronal suture ($n=7$) or at the craniotomy site after evacuation of a focal mass lesion ($n=3$). Care was taken to insert the MD catheter obliquely into the cortex using a non-traumatic technique.²⁵

We used 71 High Cut-Off Brain MD catheters with a membrane length of 10 mm and a 100 kDa nominal molecular weight cut-off polyarylethersulfone (PAES) membrane (M Dialysis AB, Solna, Sweden). The outflow hydrostatic pressure of the perfusion system was set at the zero midcranial reference level by taping the collecting vials at the bandage on the patient's head to avoid additional hydrostatic effects on fluid recovery of the catheter. Perfusion of the catheters was performed using artificial cerebrospinal fluid (CSF) (Perfusion Fluid CNS, M Dialysis), containing NaCl 147 mM, KCl 2.7 mM, CaCl₂ 1.2 mM, and MgCl₂ 0.85 mM with the addition of 1.5% human serum albumin,²⁶ at a rate of 0.3 μ L/min using a 106 MD pump (M Dialysis). At least 2 h passed after insertion of the MD catheter and start of sampling to allow for normalization of changes caused by catheter insertion. MD vials (~18 μ L samples) were changed hourly. Samples were analyzed at the bedside using CMA microdialysis analyzers (CMA600 and ISCUSflex; M Dialysis) for concentrations of glucose (MD-glc), lactate (MD-lac), and pyruvate (MD-pyr), and the LPR was calculated. Glutamate (MD-glut) and glycerol (MD-glyc) were analyzed later (CMA600). Urea was monitored to control the MD catheter performance.⁵² The remaining samples were stored at

–70°C until further analyzed for A β peptides (described subsequently). The CMA 600 Analyser was automatically calibrated when started, as well as every 6th h using standard calibration solutions from the manufacturer (M Dialysis). Quality controls at two different concentrations for each substance were performed every weekday (CMA600 and ISCUSflex). The correlation between CMA600 and ISCUSflex data from separate runs with the same control sample was found to be excellent (for all analytes used here r was ≥ 0.99) allowing for direct comparison of patient data from both instruments. Imprecision values for between assay coefficient of variation was < 10% for all analytes. The location of the MD catheter was evaluated on follow-up CT scans in all patients and checked for hemorrhages. The presence of any hemorrhage visible on TBI within 3 cm of the MD probe was analyzed on all CT scans and noted in Table 2.

Based on previous data,^{53,54} the following values for the routine biomarkers were considered critical: MD-glc < 1 mmol/L; LPR > 30; MD-lac > 3.8 mmol/L; MD-pyr < 120 μ mol/L; MD-glut > 15 μ mol/L; MD-glyc > 100 μ mol/L.

Analysis of A β peptides

After bedside analysis, the remaining hourly microdialysis samples (~14 μ L) were pooled into 2 h fractions. A β 42 and A β 40 levels were measured using the INNO-BIA A β forms assay (Innogenetics, Ghent, Belgium), which is a multiplex microsphere-based Luminex xMAP technique. In this assay, the monoclonal antibodies 21F12 and 2G3, which specifically bind A β peptides ending at Ala42 and Val40, respectively, were used as capture antibodies, and the monoclonal antibody 3D6, which specifically binds A β peptides starting at Asp1, was used as detector antibody.⁵⁵ All samples were analyzed in the presence of a mild detergent in the kit, which makes most of the A β accessible to the antibodies, although without using denaturing extraction protocols. Because of the small sample volume available, all samples were diluted 15-fold before analysis. The lowest standard point was 15 pg/mL for A β 40 and 5 pg/mL for A β 42. The lowest reported levels were set to half the value of the lowest standard point, which after correction for dilution gives a cutoff of 112 pg/mL for A β 40 and 37 pg/mL for A β 42. All analyses were performed by experienced and board-certified laboratory technicians. Serial samples from the same patient were analyzed on the same plate. Intra- and inter-plate coefficients of variation were below 10%.

TABLE 2. RADIOLOGICAL ANALYSIS OF THE WORST CT SCAN DURING THE COURSE OF THE DISEASE (SEE TEXT AND SERVADEI ET AL.⁵⁰ FOR DETAILS)

Case no.	Group	Marshall classification	Lesion type	Hematoma vol (mL)	tSAH ^a	Midline shift (mm)	IVH	Basal Cisterns ^b	Hematoma location/MD probe location
1	Focal/mixed	EML	ICH & SDH	51.4	+	7.5	+	2	RF/RF cranio ^c
2	DAI	DI II	Cps	3.5	SF +++	None	None	0	RFP/RF
3	DAI	DI II	Cps	<0.1	BP +++	None	++	0	LBG/RF
4	Focal/mixed	EML	EDH	24.9	None	4.5	None	1	RFP/RF cranio ^c
5	DAI	DI III	Cps	<0.1	LTP +	None	++	1	LF/RF
6	Focal/mixed	non-EML	Cps	10.0	BFP +++	None	None	1	LF/RF
7	Focal/mixed	EML	EDH	54.9	BSF +	2.0	None	2	LT/RF cranio
8	DAI	DI III	Cps	0.3	SF +	None	+	1	LBG/RF ^c
9	Focal/mixed	non-EML	ICH & SDH	17.8	Tent. +++	None	None	0	Bilat/F
10	DAI	DI II	Cps	0.6	Occ, +	none	++	0	RT/RF*

^aSemiquantitative scale; + = minimal, localized SAH; +++ = marked, widespread SAH.

^bScores defined as follows: 0 = normal, 1 = compressed yet visible, 2 = compressed.

^cMD probe placed within 3 cm of a CT-verified hemorrhage/contusion.

DAI, diffuse axonal injury; Cps, parasagittal contusions; cranio, craniotomy; DI II/III, diffuse injury⁵¹; EML, evacuated mass lesion; IVH, intraventricular hemorrhage; bilat., bilateral; BG, left basal ganglia; F, frontal; T, temporal; Tent, tentorium; FP, frontoparietal; Occ, occipital; tSAH, traumatic subarachnoid hemorrhage.

Statistical analysis

The microdialysis data was analyzed using the one sample Kolmogorov–Smirnov test and was found not to meet the assumption of normal distribution ($p < 0.05$ for all analytes). Therefore, pairwise comparisons between groups were analyzed using the Mann–Whitney U test (Statistica software; StatSoft, Tulsa, OK). Nonparametric data are presented as medians and 75th percentile or individual values, whereas parametric data are presented using the means \pm standard deviations (SD). Correlation analysis was performed on the first 48 h MD samples using Spearman's rank correlation. For area under the curve (AUC) calculations, we focused our analysis on the initial 19–146 h (day 1–6) post-injury. A p value < 0.05 was considered statistically significant.

Results

Patient characteristics and radiology

The mean age of the patients was 38.5 ± 18 years (range 18–76 years). The median GMS score on arrival in our NCC unit was 4 (range 2–6). Additional clinical characteristics including the NISS score are presented in Table 1. Based on the Marshall classification, the patients were divided into two groups: focal/mixed and DAI (Table 2). Five patients were categorized as having a DAI and five were categorized as having a focal/mixed injury. Radiological characteristics of each patient are presented in Table 2. Focal mass lesions were surgically evacuated in three patients (1, 4, and 7; Table 2).

Microdialysis procedure

The mean duration from time of accident to start of MD sampling was 19.7 h (range 7–75 h), and the mean duration was 179.9 ± 81 h (range 45–329 h; Table 1). Probe function was monitored using MD-urea levels, which were found to be stable, thus indicating adequate probe function, with a gradually increasing trend during the course of the monitoring period as previously shown.⁵² Less than one percent of urea samples showed deviating levels from the expected trend, leading to exclusion of all MD data during that hour. No signs of hemorrhage around the MD probe were seen on any of the control CT scans.

Interstitial $A\beta_{40}$ and $A\beta_{42}$ levels

We were able to detect $A\beta_{40}$ and $A\beta_{42}$ in 2 h MD samples for all 10 patients using the Luminex method.⁵⁵ In total, 1530 MD samples were analyzed for both markers ($n = 765$ samples for each marker).

All together, the interstitial $A\beta_{40}$ and $A\beta_{42}$ levels were only slightly variable, with minor fluctuations during the course of the disease (Fig. 1A and B). We hypothesized that the $A\beta$ levels were related to injury type, energy metabolic situation, age of the patient, and/or the level of consciousness.

First, we compared the $A\beta$ peptide levels in relation to injury type (Fig. 1A–D).

Including all MD samples, the median interstitial $A\beta_{40}$ levels were 782 pg/mL (range 457.0–971.3 pg/mL) and 436 pg/mL (range 281.3–766.5 pg/mL) in the DAI and focal TBI groups, respectively. $A\beta_{42}$ levels were 106 pg/mL (range 62–127.5 pg/mL) and 60 pg/mL (range 46–90 pg/mL) in the DAI and focal TBI group, respectively. The $A\beta$ peptide levels were consistently higher in the patients with DAI than in patients with a focal TBI, being statistically significant for $A\beta_{42}$ at 113–116 h post-injury ($p < 0.05$; Fig. 1A and B). Area under the curve (AUC), calculated from 19–146 h post-injury, was also compared (Fig. 1C and D). The AUC in the

DAI group tended to be higher than the total AUC in the focal injury group (Fig. 1C and D), although without reaching statistical significance. For all samples, there was a strong correlation between interstitial $A\beta_{40}$ and $A\beta_{42}$ levels ($r = 0.987$; Fig. 1E) and no association of the $A\beta_{42}/A\beta_{40}$ ratio with any of the outcome parameters was observed (data not shown).

We hypothesized that the energy metabolic situation could influence $A\beta$ levels, and we performed a correlation analysis between the low molecular weight (LMW) biomarkers and $A\beta$ -peptide levels (Fig. 2A–D). However, $A\beta$ levels only weakly correlated with the evaluated biomarkers for cerebral ischemia (shown for the LPR ($r = 0.40$ and $r = 0.41$ for $A\beta_{40}$ and $A\beta_{42}$, respectively; $p < 0.05$) in Fig. 2A and B, MD-glc ($r = 0.76$ and $r = 0.77$ for $A\beta_{40}$ and $A\beta_{42}$, respectively; $p < 0.05$) in Fig. 2C and D and for MD-pyr ($r = 0.13$ for both $A\beta_{40}$ and $A\beta_{42}$, $p = \text{n.s.}$, data not shown; not shown for MD-glut, MD-glyc and MD-lac). MD-glut ($r = 0.755$ and $r = 0.735$, respectively) and MD-glyc ($r = 0.45$ and $r = 0.84$) was weakly correlated to interstitial $A\beta_{40}$ and $A\beta_{42}$ levels (data not shown). The LPR was frequently higher early and MD-glyc was higher late following the injury in patients with a focal TBI than in patients with diffuse TBI ($p < 0.05$, Fig. 6A) without other significant differences in energy metabolic markers depending upon injury type or age of the patient. We then evaluated the influence of age on $A\beta$ levels, divided into two groups (< 40 and > 40 years old). Age did not significantly influence our $A\beta$ peptide results (Fig 3A–D). There was no correlation between the clinical outcome evaluated using the extended Glasgow coma outcome scale (eGOS) and the $A\beta$ peptide levels (data not shown).

Five patients never obeyed command during the monitoring time (deemed unconscious) evaluated by the neurological wake-up test, five did (deemed conscious), and we next analyzed the effect of level of consciousness on $A\beta$ peptide levels.²⁶ The levels of $A\beta_{40}$ and $A\beta_{42}$ were not significantly influenced by the level of consciousness (Fig. 4A–D) nor was there a correlation between $A\beta$ and LPR or MD-glc (data not shown). Additionally, the frequent neurological wake-up tests did not markedly alter $A\beta_{40}$ and $A\beta_{42}$ levels (for an illustrative patient example see Fig. 5). In most patients, there were only slight fluctuations in $A\beta_{40}$ and $A\beta_{42}$ levels. One patient in the DAI group (case 8, Fig. 4) had very high $A\beta$ levels (Fig. 5).

Analyses of low-molecular weight MD markers

LPR. A total of 1582 MD samples could be analyzed for the LPR. LPR levels were significantly higher early post-injury in the focal injury group (Fig. 6A). Age (Fig. 6B) and the level of consciousness (data not shown) did not influence the LPR levels.

MD-glc. A total of 1582 MD samples were analyzed for glucose (MD-glc). Of these, 179 samples (11.3%) had a critical MD-glc value of < 1 mmol/L. Injury type (Fig. 6A), age (Fig. 6B), and level of consciousness (data not shown) did not significantly influence MD-glc levels.

MD-glut. We could analyze 1302 samples for glutamate (MD-glut). The MD-glut values did not markedly differ between the injury groups (Fig. 6A) and was not influenced by the level of consciousness (data not shown). In young patients, MD-glut levels were consistently higher mainly because of one young patient with high MD-glut levels (Fig. 6B).

MD-glyc. We could analyze 1657 samples for glycerol (MD-glyc). When compared with the focal TBI group, patients with diffuse TBI had consistently lower MD-glyc values ($p < 0.05$ in

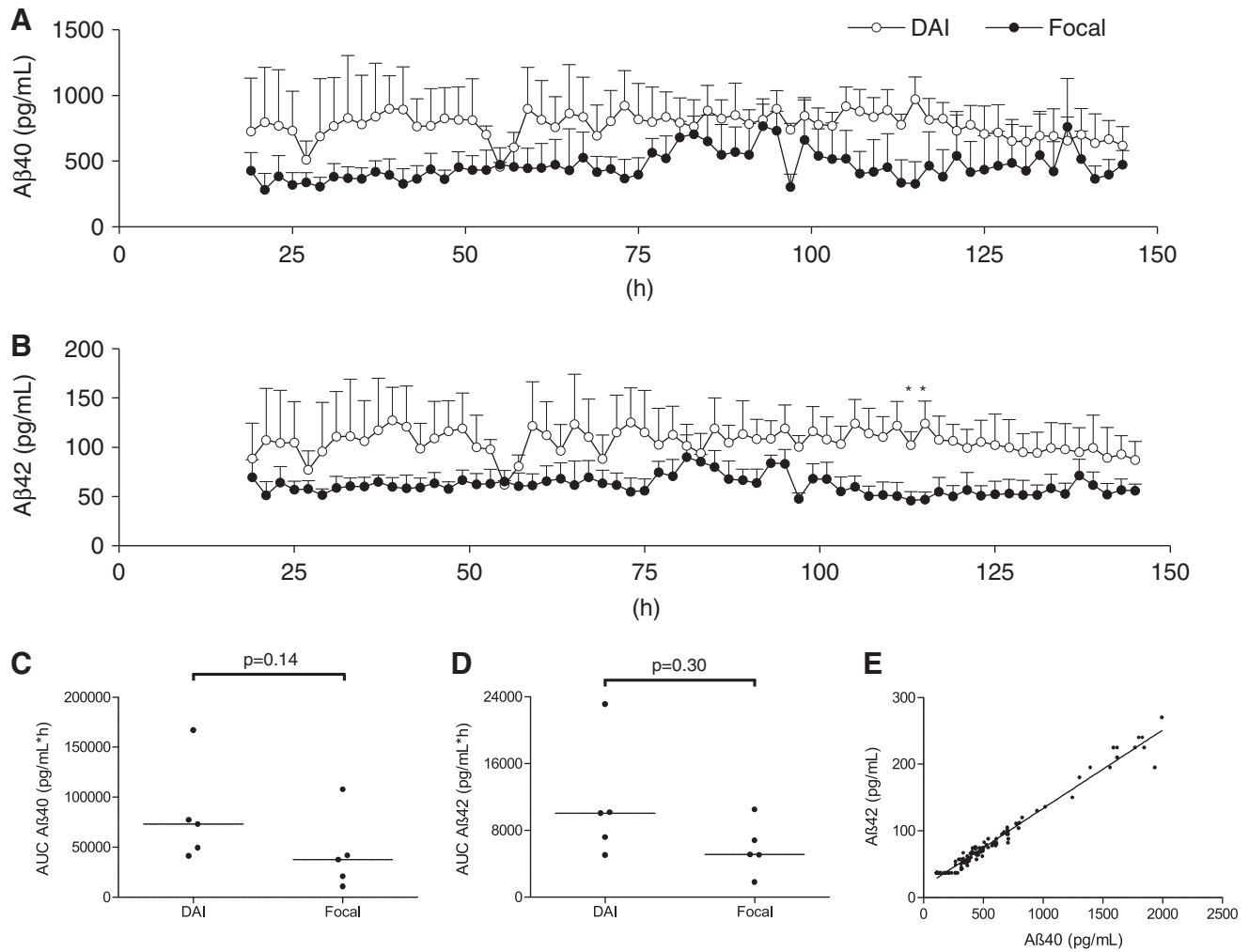


FIG. 1. Interstitial amyloid- β ($A\beta$)40 (**A**) and $A\beta$ 42 (**B**) concentrations were determined in 2 h sample fractions. For clarity, the data are presented as means \pm SEM. Patients with diffuse axonal injury (DAI) (open circles) had consistently higher values than patients with mixed/focal traumatic brain injury (filled squares). A significant difference (<0.05) is indicated with an *. (**C–D**) Area under the curve (AUC) values for each patient in the DAI (five patients) and mixed/focal (five patients) TBI groups. The AUC value for each patient was calculated for $A\beta$ 40 (**C**) and $A\beta$ 42 (**D**) between 19 and 146 h post-injury, presented with the median value (black line) and the individual values. (**E**) There was a very strong correlation between the $A\beta$ 40 and $A\beta$ 42 levels in the microdialysis (MD) samples.

8/12 samples from 111 to 123 h post-injury; Fig. 6A). Age (Fig. 6B) or the level of consciousness (data not shown) did not significantly influence the MD-glyc levels.

Discussion

The aim of this study was to evaluate the dynamics of the $A\beta$ peptides $A\beta$ 40 and $A\beta$ 42 after TBI using intracerebral MD. The refined analysis method allowed for monitoring of both $A\beta$ 40 and $A\beta$ 42 in 2 h fractions in a small but thoroughly characterized TBI cohort. These results provide a unique data set for evaluation of $A\beta$ peptide dynamics in the acute phase following injury, with higher temporal resolution and analytical specificity than in previously published studies.^{25,26,45} The $A\beta$ results were also compared with injury type, biomarkers for cerebral energy metabolism (glucose, lactate, pyruvate), cellular distress (glycerol, and glutamate), and clinical factors including patient age and level of consciousness, to test our main hypotheses. Higher $A\beta$ levels in patients with diffuse brain injury compared with focal TBI were observed, supporting

our previous data suggesting that $A\beta$ peptides may be valuable biomarkers for axonal injury.²⁵ In contrast, the energy metabolic situation evaluated using MD biomarkers of ischemia and cellular distress in the same brain region only weakly correlated with $A\beta$ peptide levels. Additionally, patient age or level of consciousness did not clearly influence $A\beta$ levels in this patient cohort.

We observed that the levels of the $A\beta$ peptides $A\beta$ 40 and $A\beta$ 42 were higher in patients with diffuse brain injury than in those with focal TBI, and there are several lines of evidence suggesting an increased $A\beta$ formation following diffuse TBI. First, in approximately one third of TBI patients, $A\beta$ plaques have been detected in the postmortem brain,⁵⁶ in surgically resected tissue,^{11,12} and in injured axons of DAI patients dying <9 days post-injury.¹⁴ This TBI-induced $A\beta$ pathology can remain for many years in the brains of TBI survivors.^{5,57} Second, following diffuse TBI in the pig, $A\beta$ plaques were observed in the one third of animals displaying the most severe axonal injury.⁵⁸ Importantly, such plaques occur not only in cortical tissue but also in white matter tracts.¹⁴ Finally, axonal accumulation of $A\beta$, APP, and BACE has been observed in

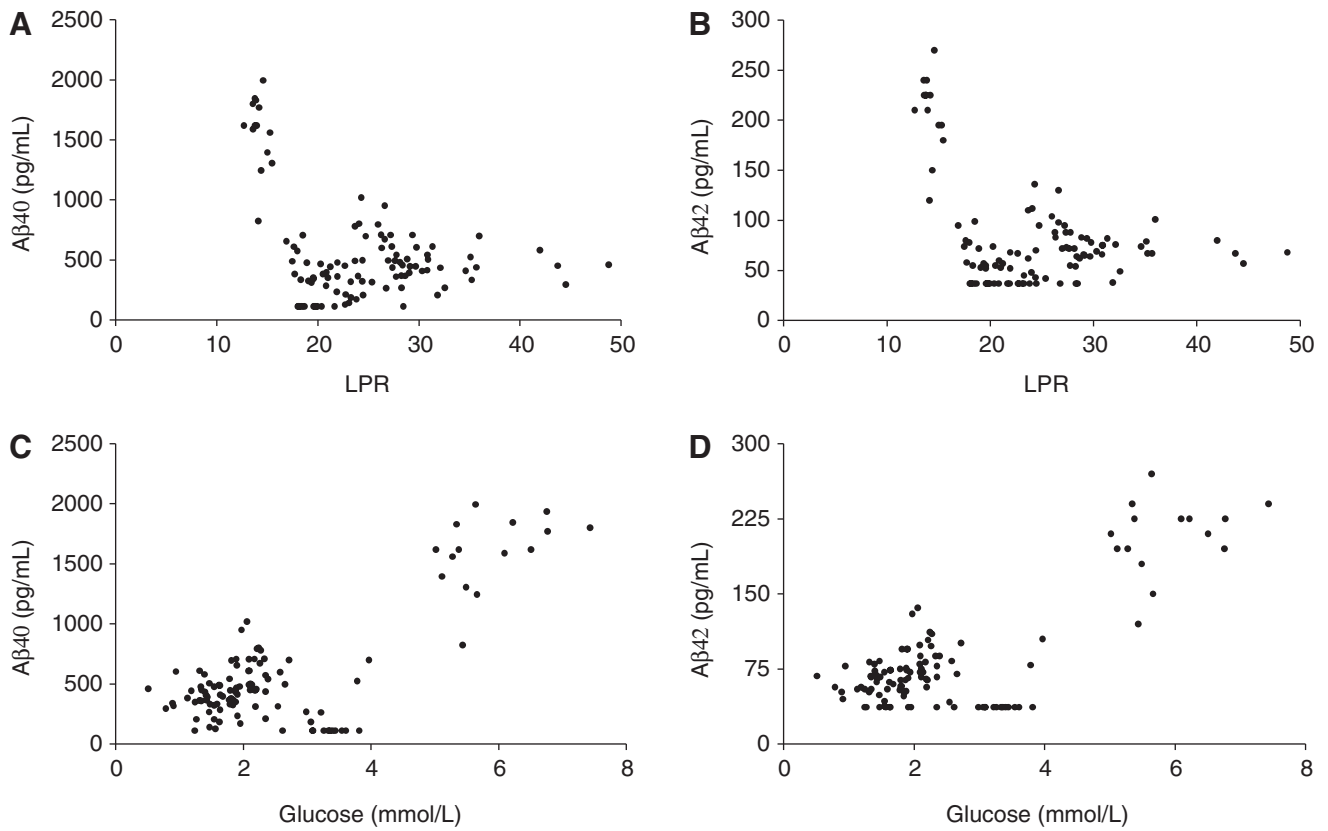


FIG. 2. We correlated amyloid- β ($A\beta$)40 (**A,C**) and $A\beta$ 42 (**B,D**) to the lactate-pyruvate ratio (LPR; **A,B**), where an LPR >30 was considered critical and to microdialysis (MD)-glucose levels (**C,D**), where a level <1.0 mmol/L was considered critical. We used the initial 48 h post-injury values and no correlation was found between $A\beta$ 40 or $A\beta$ 42 and LPR or any other marker of energy metabolic crisis.

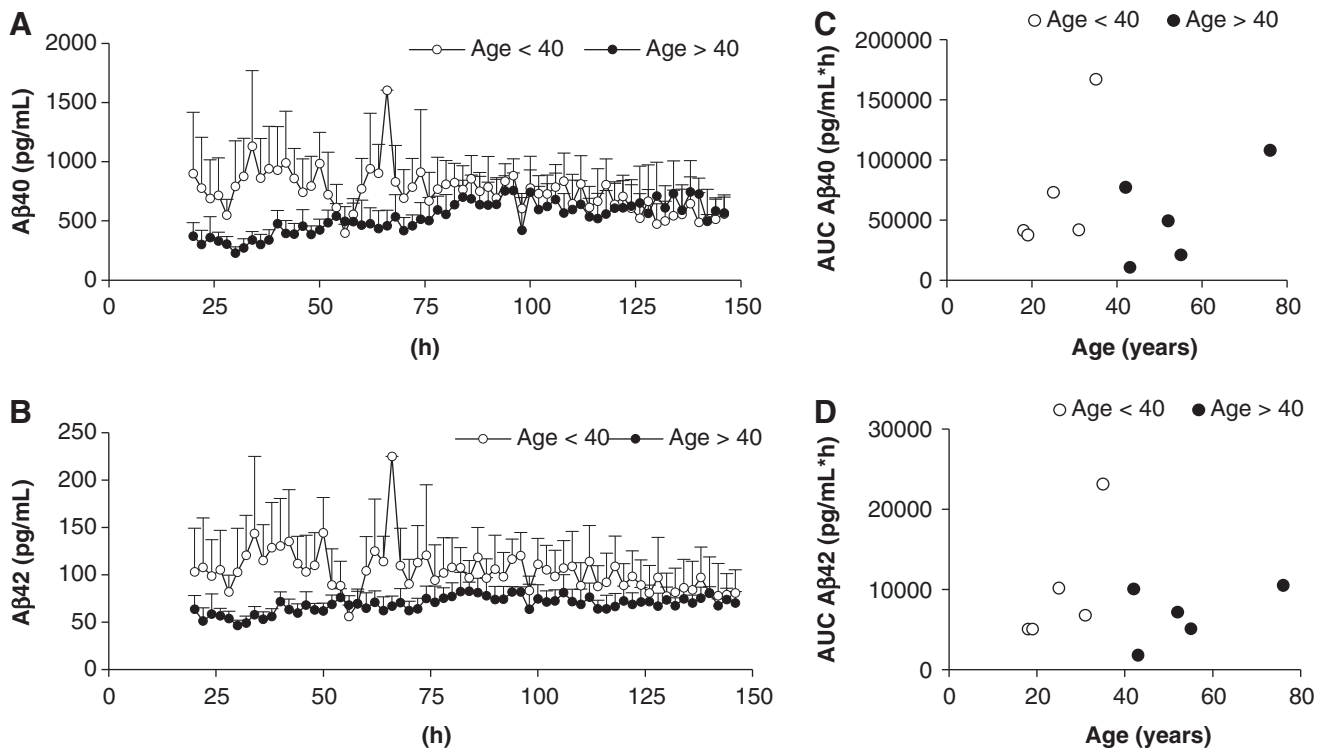


FIG. 3. We analyzed the influence of age on amyloid- β ($A\beta$)40 (**A,C**) and $A\beta$ 42 (**B,D**) levels. Open circles represent the five patients <40 years of age and filled squares represent the five patients >40 years of age. Data are presented using means \pm SD. (**C,D**) Area under the curve (AUC) $A\beta$ 40 and $A\beta$ 42 values, calculated for each traumatic brain injury (TBI) patient between 19 and 146 h post-injury and presented for patients <40 years (five patients, open circles) and >40 years old (five patients, filled squares). (**A-D**) Age defined as < or > 40 years old did not significantly influence $A\beta$ levels.

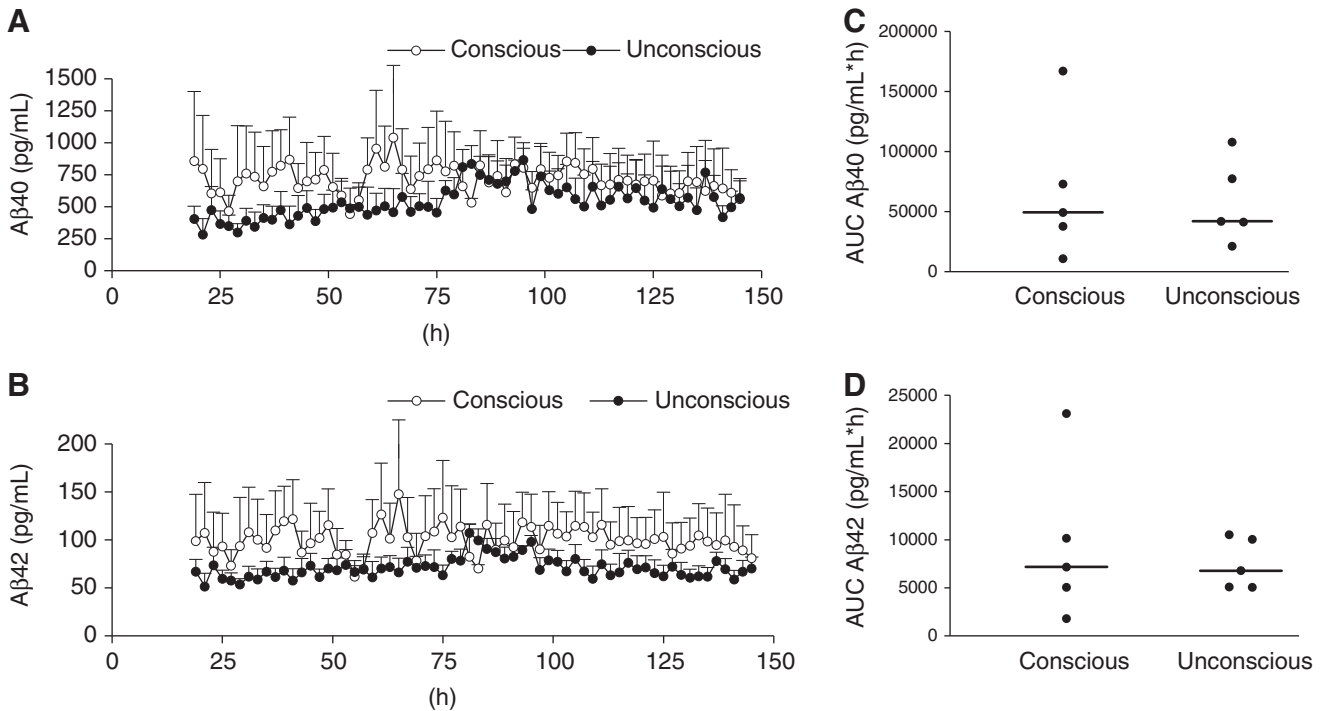


FIG. 4. (A,B) We evaluated the relationship between the level of consciousness and the interstitial amyloid- β ($A\beta$)40 (A) and $A\beta$ 42 (B) values, data presented as means \pm SD. $A\beta$ levels were similar in conscious patients (defined as patients obeying command when assessed using the neurological wake-up test; open circles) or unconscious patients (filled squares). (C,D) Area under the curve (AUC) values for each patient in the conscious and unconscious groups. The AUC value for each patient was calculated for $A\beta$ 40 (C) and $A\beta$ 42 (D) between 19 and 146 h post-injury, presented with the median value (black line) and the individual values. There were no significant differences among the groups.

both human and pig DAI up to 3 years post-injury.^{21,22,59} Therefore, it appears likely that a prolonged APP accumulation in swollen axons results in an increased formation of $A\beta$ peptides^{5,56,60} released into the interstitial compartment following axonal rupture.

It should be noted that the classification of focal TBI versus DAI was solely based on the Marshall classification of CT scans, which is based on a 1991 analysis of the Traumatic Coma Data Bank. Although this classification was found to be predictive of a poor outcome, its ability to predict detailed neuropsychological deficits has not been established.⁶¹ MRI is clearly more sensitive than CT for small lesions such as those observed in DAI patients.⁶² In our material, no patient in the DAI group had a focal lesion, and the largest hematoma in this group was <4 mL. However, with ever increasing sensitivity of MRI, it is becoming clear that a high proportion of patients with predominately focal TBI display components of axonal injury.⁶³ As standard CT and MRI may underestimate the extent of white matter damage after TBI,^{64,65} additional neuroradiological tools such as diffusion tensor imaging (DTI) could further increase the detection of white matter damage post-injury.⁶⁶ Ideally, MR scans following the implantation of the MD catheters could in more detail have evaluated the details of axonal injury in the vicinity of the probes in our present study.

The $A\beta$ 40 and $A\beta$ 42 levels did not markedly fluctuate during the initial post-injury days following human TBI, in contrast to previous MD studies in which they gradually rose over time.^{26,45} Our observations are also in contrast to experimental data analyzing $A\beta$ levels using MD early following focal TBI in mice. In awake, moving mice, the hippocampal $A\beta$ levels declined by up to 50% post-injury, depending upon injury severity. In animals with severe TBI, the $A\beta$ decline was more marked and prolonged than in animals

with a milder, focal TBI.⁶⁷ In the present series, the pre-injury levels were unknown, and initial $A\beta$ levels may have been different. It is likely that human TBI represents a less marked focal TBI than what is used in the rodent model,⁶⁸ making direct comparisons difficult.

Although the evidence cited in the previous paragraphs suggest that $A\beta$ levels may be increased post-injury, we must also consider that the $A\beta$ levels presented in our study may actually be reduced in some TBI patients.⁴⁵ In a previous study, patients with contusions had lower $A\beta$ peptide levels than did DAI patients,^{26,45} findings similar to our present and previous report.²⁵ In our focal TBI group, three patients had their MD probes close to an evacuated mass lesion, and the lower values observed in the focal TBI group may also represent reduced levels in the vicinity of contusion caused by $A\beta$ consumption in the formation of plaques. Although the lack of histology makes any explanation hypothetical, early plaque formation is observed in only one third of TBI patients (see earlier description). Therefore, it is unlikely that the reduced $A\beta$ levels in focal TBI patients are the result of plaque formation. Although CSF $A\beta$ concentration may differ from the interstitial concentration,⁵ levels of $A\beta$ 42 have been reported to increase following TBI.^{60,69–72}

Any biomarker may also have an effect on the injury process itself. Based on experimental data, interstitial $A\beta$ may have deleterious effects following TBI.²⁴ Neurotoxic and synaptotoxic effects of $A\beta$ oligomers *per se* have also been observed.^{42–44} Therefore, the interstitial $A\beta$ could influence the secondary injury cascade after TBI. In addition, alternate splicing of the APP molecule may occur, and generation of other $A\beta$ species than $A\beta$ 42 evaluated in our present report is possible. The shorter $A\beta$ 1–40 ($A\beta$ 40) makes ~ 80 – 90% of all generated $A\beta$ peptides, although $A\beta$ 42 is more hydrophobic and prone to aggregate into plaques.²⁶ In

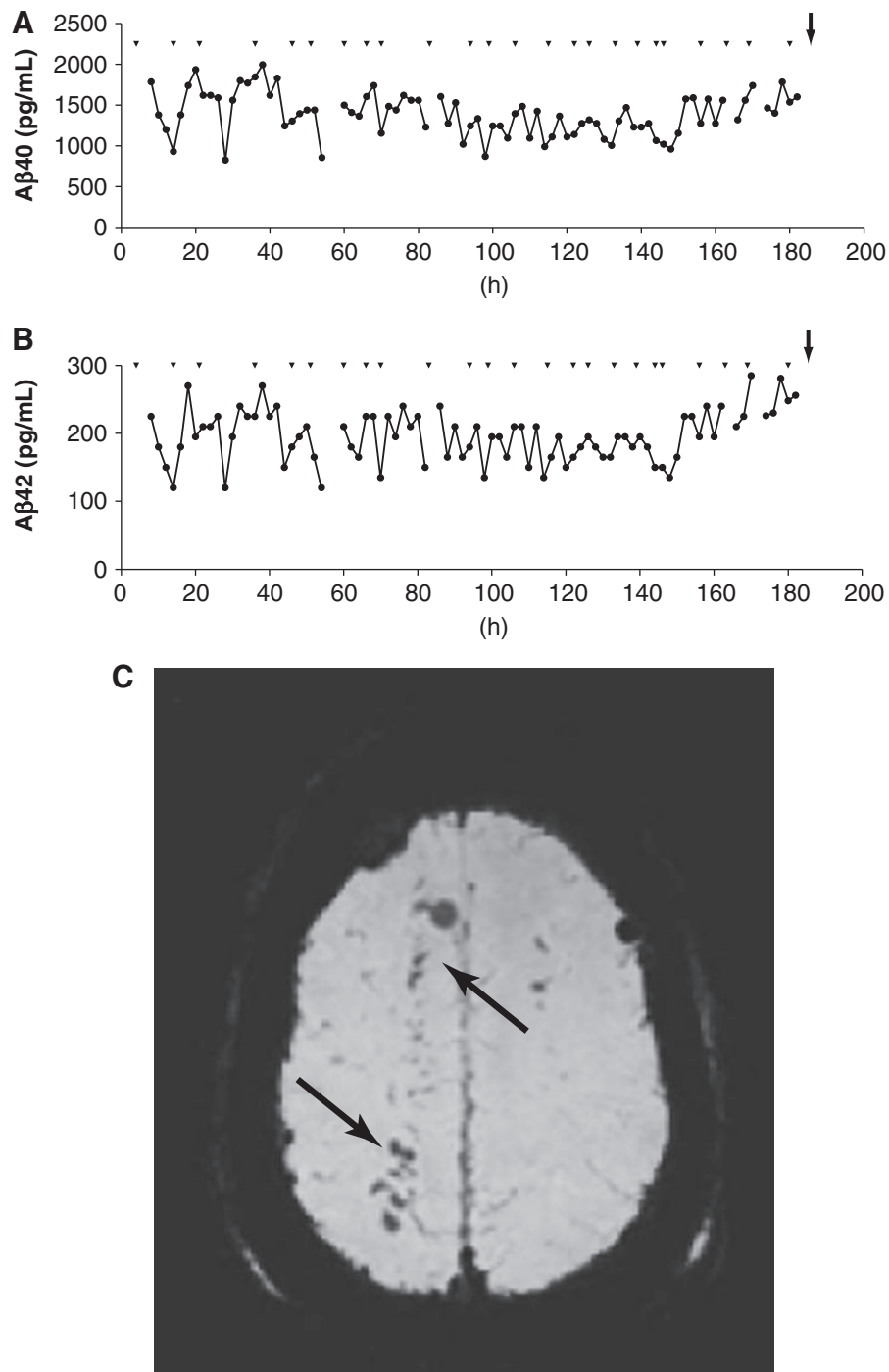


FIG. 5. Microdialysis data from a patient who sustained a Marshall diffuse brain injury II traumatic brain injury after a fall during horseback riding. Graph showing changes in amyloid- β ($A\beta$)40 (**A**) and $A\beta$ 42 (**B**) levels detected using microdialysis. (**C**) An MR scan obtained at 2 days post-injury showing multiple hemorrhages at the gray–white matter interface, indicated with arrows, suggestive of diffuse axonal injury (DAI). The highest interstitial $A\beta$ 40 and $A\beta$ 42 levels of this patient series were observed in this patient. Despite gradually improving neurological status during the monitoring time, the $A\beta$ did not change and remained at a high level. The time for interruption of sedation in order to evaluate the level of consciousness using the neurological wake-up test, shown with arrowheads, did not clearly influence $A\beta$ levels. The time for extubation is shown with an arrow.

the pathophysiology of TBI, other $A\beta$ subspecies than $A\beta$ 42 may be of interest, which could be evaluated using MD.⁷³ The cutoff for the MD catheter used in the present study was 100 kDa, and although the molecular weight of $A\beta$ 42 is \sim 4.5 kDa, longer peptides resulting from APP splicing or $A\beta$ oligomerization, presumably a key event in the pathogenesis of AD, may not be detected using MD.⁷⁴

As cerebral ischemia may influence $A\beta$ levels,^{34–36} we evaluated biomarkers for energy metabolic perturbation obtained in the same location and brain compartment as $A\beta$. In contrast to a previous report,²⁶ which found a positive correlation between MD- $A\beta$ and MD-glc and a negative correlation with LPR, we observed only weak correlations. In our series, pathological LPR and/or MD-glc

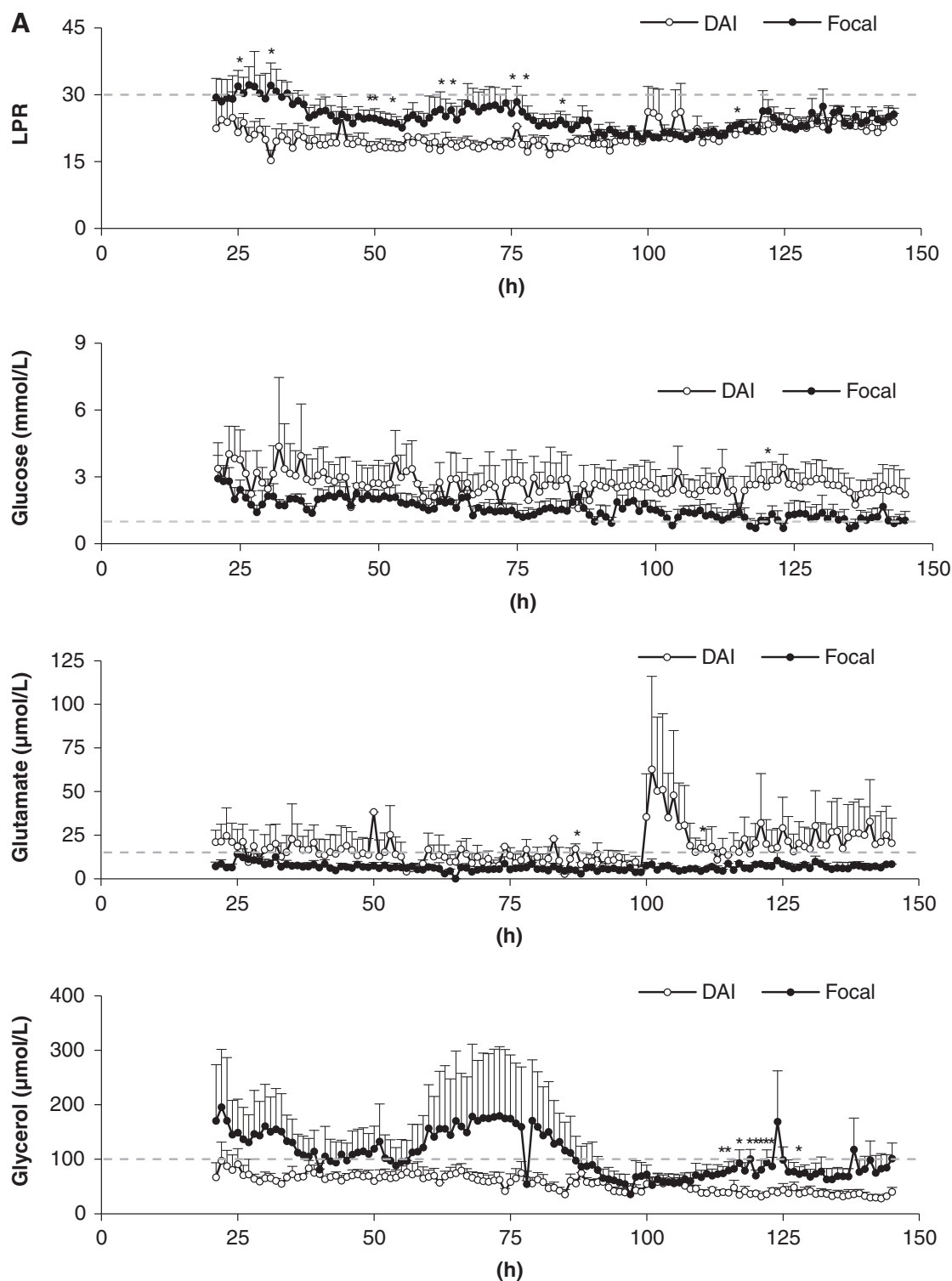


FIG. 6. A,B. Interstitial lactate-pyruvate ratio (LPR), glucose, glutamate and glycerol measured using microdialysis (MD), data presented as means \pm SD. The energy metabolic markers showed similar values when the patients were divided into groups depending on injury type (A) and age (B). (A) Graph showing the LPR, MD-glucose, MD-glutamate, and MD-glycerol levels in the diffuse axonal injury group (DAI; open circles) compared with the focal injury group (filled squares) in MD samples from 21 to 145 h post-injury. Significant differences between the two groups indicated with an asterisk (*). (B) The energy metabolic situation, analyzed showing the LPR and MD-glucose in five patients >40 years old compared with the younger patients <40 years old. No significant differences were seen between the two groups. The dashed lines in A and B indicate critical cut-off levels for the LPR (>30), MD-glucose (<1.0 mmol/L), MD-glutamate (18 $\mu\text{mol/L}$) and MD-glycerol (100 $\mu\text{mol/L}$).

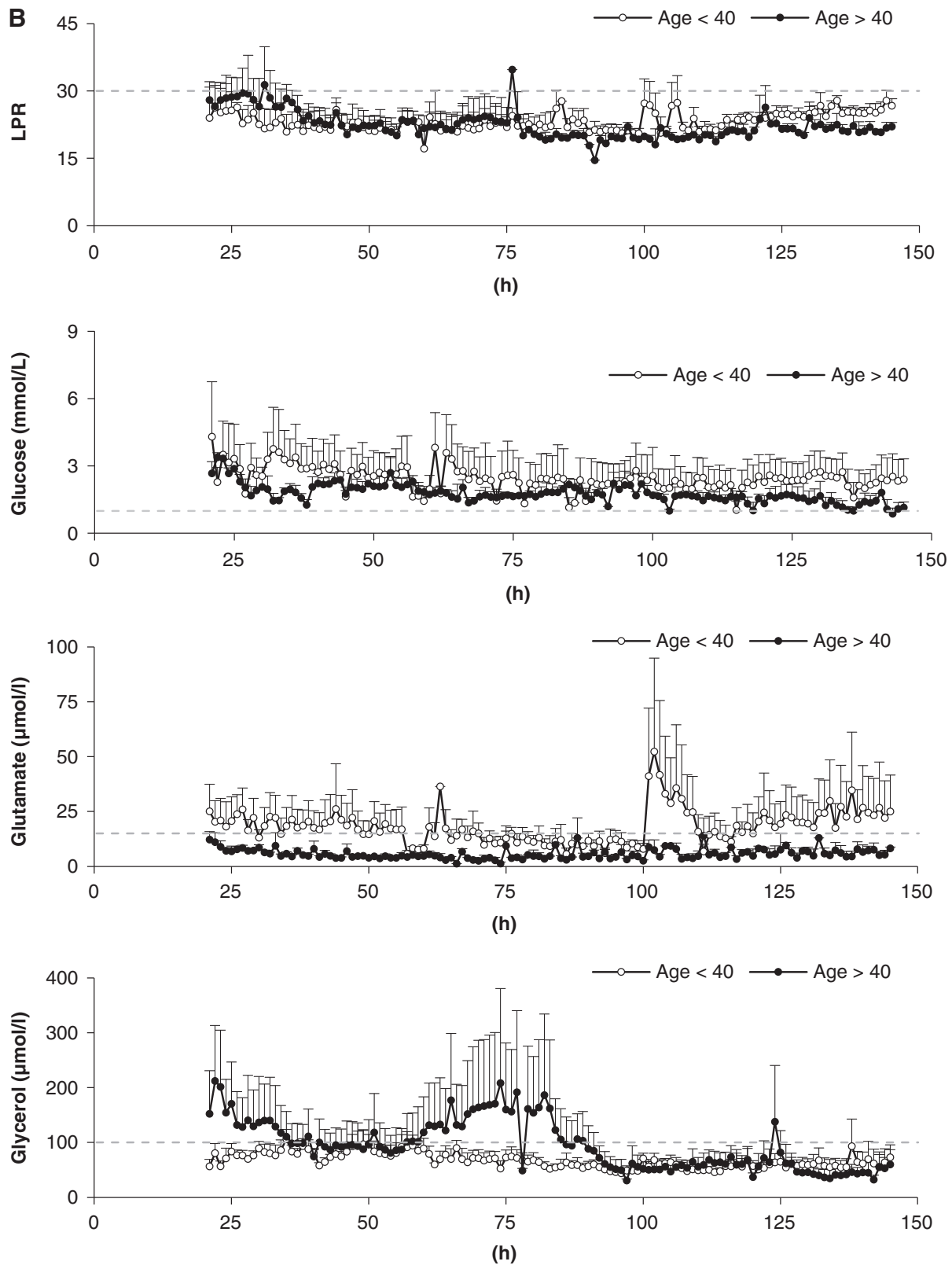


FIG. 6. (Continued)

values were rather infrequent and, at least for MD-glc, appeared less frequently than in the study by Brody and associates.²⁶ Additionally, in that report, six patients with subarachnoid hemorrhage (SAH) were included, and it cannot be excluded that those patients had a different neurochemical profile. The patients in our series had a severe TBI requiring sedation and controlled ventilation. Despite the injury severity, ICP problems were rare, which likely prevented marked neurometabolic perturbation of the brain. It cannot be excluded that another injury severity may have caused a different correlation between A β peptide levels and the focal neurochemistry.

Previously, currently available ELISA methods were considered too insensitive to enable measurement of A β 1–42 levels, and in a previous report, an ELISA evaluating A β species from amino acid 1–28 or greater (A β 1– x) was used.²⁶ When using that analysis, the majority of the A β was neither A β 40 nor A β 42, and it was suggested that A β 40 and A β 42 concentrations were lower than the A β 1– x concentrations by a factor of 35 and 2.5, respectively.²⁶ In our previous study, a high sensitivity variant of a commercially available ELISA kit was used.²⁵ In 12 h pooled samples, we were able to analyze A β 40 in ~50% of the patients, and were able to analyze A β 42 in seven out of eight patients. These levels were comparable to those obtained in the present report. However, in the present report, the analysis of A β 40 and A β 42 in 2 h samples was possible in all patients, indicating a superior sensitivity using the microsphere-based Luminex xMAP technique. The high specificity of the antibodies used in the present report and their application in the Luminex technique has previously been established.^{75–77} As long-term storage of CSF and plasma samples was found to influence the analysis of A β ,^{78,79} consideration of pre-analytical factors was crucial. Prior to analysis, the MD samples in our present study were stored at –70°C, and every precaution was taken to handle and store the samples properly. We believe that the minor fluctuations of A β during the course of the disease for the individual patient reflected this effort. In addition, the MD membrane may serve as a barrier separating A β from degrading enzymes such as insulinase and neprilysin,⁸⁰ contributing to sample stability. Finally, other groups have observed long-term stability of A β in CSF samples for >2 years of freezing,^{81,82} arguing that pre-analytical factors did not markedly influence our results. However, further studies are clearly needed to define the effect of pre-analytical factors such as long-term storage on analyte levels.

Although astrocytes, microglia, and endothelial and smooth muscle cells may release A β , neurons express the highest levels of APP and may release A β into the extracellular space under normal cellular conditions.⁸³ In one previous report using MD, the A β levels were dependent on the level of consciousness.²⁶ In that report, studying a mixed TBI and SAH cohort, A β levels rose when the patient's neurological status improved and vice versa. Here, we did not detect a similar correlation among A β 40, A β 42, and the level of consciousness in a pure TBI cohort. As an important part of routine NCC monitoring, we frequently evaluate the neurological status (the motor component of the GCS), using the neurological wake-up test⁴⁶ requiring that the continuous sedation be interrupted. Despite the absence of sedation during the tests, interstitial A β levels were not markedly altered. There are several experimental reports suggesting a link between extracellular A β dynamics and neuronal activity.^{83–86} It is plausible that TBI-induced factors are responsible for regulating neuronal activity and, conversely, A β levels. The wake-up test and reduction of sedation may not be sufficient to overcome TBI-induced depression of neuronal activity. In addition, the neurological evaluation performed in the

NCC setting provides only a crude measurement of neuronal activity, and may be influenced by many additional factors other than TBI severity. Therefore, the lack of correlation between A β levels measured using MD and the level of consciousness observed here may not be surprising. However, as there was a lack of pre-injury, baseline A β levels in the present data cannot resolve the possibility that our findings were the result of increased A β caused by axonal injury or a larger decrease in A β levels in focal TBI caused by a more marked regional decrease in neuronal activity. In addition, A β oligomers and protofibrils could be elevated after TBI, despite a reduction in MD A β levels. These issues should be addressed in future studies.

Limitations

There are obvious limitations to our study. The present cohort of 10 TBI patients is small, which may have prevented us from detecting significant correlations between A β levels and a number of clinical and radiological factors. Because of the heterogeneity of TBI, this number may be insufficient to enable firm conclusions, and even though each patient was thoroughly characterized, additional studies are needed. A routine use of MR imaging would more accurately have been able to determine the pathology and presence of axonal injury in the vicinity of the MD probe. Additionally, multimodal monitoring of each patient including electroencephalogram (EEG) and brain tissue oxygenation combined with, for example, positron emission tomography (PET) monitoring could have strengthened the interpretation of energy metabolic changes in relation to MD A β levels. The A β peptides evaluated in the present report may be relevant in the acute pathophysiology of TBI, and recent studies have indicated the importance of A β oligomers, not measured in the present study, in neurodegeneration.⁸⁷ Even though A β is produced by normal neuronal metabolism,⁸⁸ the normal extracellular A β levels using MD and our present analysis technique are unknown. Finally, the rates of enzymatic degradation, uptake into activated microglia, and receptor-mediated export of A β to other organs,⁷³ perhaps influenced by TBI, were not measured, and may have modulated our MD A β levels.

Conclusion

Using a microsphere-based Luminex xMAP technique, we were able to analyse and monitor A β 40 and A β 42 levels in bi-hourly samples in severe human TBI. Our data support the notion that MD is a useful tool for studying A β dynamics following TBI. We also confirm our previous hypothesis that these A β peptides occur at higher concentration in patients with diffuse injury than in those with focal TBI. However, we could not find a correlation between A β levels and the focal energy metabolic situation, biomarkers of cellular distress, age of the patient, or the patient's level of consciousness. Future studies using an increased number of TBI patients are needed to confirm these observations. Additional markers such as tau and neurofilament and/or A β subspecies including oligomers and protofibrils should also be used as previously suggested⁷³ for elucidating the potential role of A β in the pathobiology of TBI as well as the complex relationship between TBI and AD pathology.

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Author Disclosure Statement

Analysis of A β peptides were done at the time Dr. Vanmechelen was employed at Innogenetics, and results were transferred to the Institute of Neuroscience and Physiology and Division of Neurosurgery. All subsequent analyses and interpretations were done after September 2011. No other competing financial interest exists.

References

- Selassie, A.W., Zaloshnja, E., Langlois, J.A., Miller, T., Jones, P., and Steiner, C. (2008). Incidence of long-term disability following traumatic brain injury hospitalization, United States, 2003. *J. Head Trauma Rehabil.* 23, 123–131.
- McAllister, T.W. (2011). Neurobiological consequences of traumatic brain injury. *Dialogues Clin. Neurosci.* 13, 287–300.
- Zetterberg, H., Hietala, M.A., Jonsson, M., Andreasen, N., Styrd, E., Karlsson, I., Edman, A., Popa, C., Rasulzada, A., Wahlund, L.O., Mehta, P.D., Rosengren, L., Blennow, K., and Wallin, A. (2006). Neurochemical aftermath of amateur boxing. *Arch. Neurol.* 63, 1277–1280.
- McKee, A.C., Stein, T.D., Nowinski, C.J., Stern, R.A., Daneshvar, D.H., Alvarez, V.E., Lee, H.S., Hall, G., Wojtowicz, S.M., Baugh, C.M., Riley, D.O., Kubilus, C.A., Cormier, K.A., Jacobs, M.A., Martin, B.R., Abraham, C.R., Ikezu, T., Reichard, R.R., Wolozin, B.L., Budson, A.E., Goldstein, L.E., Kowall, N.W., and Cantu, R.C. (2013). The spectrum of disease in chronic traumatic encephalopathy. *Brain* 136, 43–64.
- Johnson, V.E., Stewart, W., and Smith, D.H. (2010). Traumatic brain injury and amyloid-beta pathology: a link to Alzheimer's disease? *Nat. Rev. Neurosci.* 11, 361–370.
- Plassman, B.L., Havlik, R.J., Steffens, D.C., Helms, M.J., Newman, T.N., Drosdick, D., Phillips, C., Gau, B.A., Welsh-Bohmer, K.A., Burke, J.R., Guralnik, J.M., and Breitner, J.C. (2000). Documented head injury in early adulthood and risk of Alzheimer's disease and other dementias. *Neurology* 55, 1158–1166.
- Clinton, J., Ambler, M.W., and Roberts, G.W. (1991). Post-traumatic Alzheimer's disease: preponderance of a single plaque type. *Neuropathol. Appl. Neurobiol.* 17, 69–74.
- Mortimer, J.A., Van Duijn, C.M., Chandra, V., Fratiglioni, L., Graves, A.B., Heyman, A., Jorm, A.F., Kokmen, E., Kondo, K., Rocca, W.A., et al. (1991). Head trauma as a risk factor for Alzheimer's disease: a collaborative re-analysis of case-control studies. *EURODEM Risk Factors Research Group. Int. J. Epidemiol.* 20, Suppl. 2, S28–35.
- Guo, Z., Cupples, L.A., Kurz, A., Auerbach, S.H., Volicer, L., Chui, H., Green, R.C., Sadovnick, A.D., Duara, R., DeCarli, C., Johnson, K., Go, R.C., Growdon, J.H., Haines, J.L., Kukull, W.A., and Farrer, L.A. (2000). Head injury and the risk of AD in the MIRAGE study. *Neurology* 54, 1316–1323.
- Mayeux, R., Ottman, R., Tang, M.X., Noboa-Bauza, L., Marder, K., Gurland, B., and Stern, Y. (1993). Genetic susceptibility and head injury as risk factors for Alzheimer's disease among community-dwelling elderly persons and their first-degree relatives. *Ann. Neurol.* 33, 494–501.
- DeKosky, S.T., Abrahamson, E.E., Ciallella, J.R., Paljug, W.R., Wisniewski, S.R., Clark, R.S., and Ikonovic, M.D. (2007). Association of increased cortical soluble abeta42 levels with diffuse plaques after severe brain injury in humans. *Arch. Neurol.* 64, 541–544.
- Ikonovic, M.D., Uryu, K., Abrahamson, E.E., Ciallella, J.R., Trojanowski, J.Q., Lee, V.M., Clark, R.S., Marion, D.W., Wisniewski, S.R., and DeKosky, S.T. (2004). Alzheimer's pathology in human temporal cortex surgically excised after severe brain injury. *Exp. Neurol.* 190, 192–203.
- Li, J., Li, X.Y., Feng, D.F., and Pan, D.C. (2010). Biomarkers associated with diffuse traumatic axonal injury: exploring pathogenesis, early diagnosis, and prognosis. *J. Trauma* 69, 1610–1618.
- Smith, D.H., Chen, X.H., Iwata, A., and Graham, D.I. (2003). Amyloid beta accumulation in axons after traumatic brain injury in humans. *J. Neurosurg.* 98, 1072–1077.
- Lewen, A., Li, G.L., Olsson, Y., and Hillered, L. (1996). Changes in microtubule-associated protein 2 and amyloid precursor protein immunoreactivity following traumatic brain injury in rat: influence of MK-801 treatment. *Brain Res.* 719, 161–171.
- Pierce, J.E., Trojanowski, J.Q., Graham, D.I., Smith, D.H., and McIntosh, T.K. (1996). Immunohistochemical characterization of alterations in the distribution of amyloid precursor proteins and beta-amyloid peptide after experimental brain injury in the rat. *J. Neurosci.* 16, 1083–1090.
- Nunan, J., and Small, D.H. (2000). Regulation of APP cleavage by alpha-, beta and gamma-secretases. *FEBS Lett.* 483, 6–10.
- Masters, C.L., Cappai, R., Barnham, K.J., and Villemagne, V.L. (2006). Molecular mechanisms for Alzheimer's disease: implications for neuroimaging and therapeutics. *J. Neurochem.* 97, 1700–1725.
- Blennow, K., de Leon, M.J., and Zetterberg, H. (2006). Alzheimer's disease. *Lancet* 368, 387–403.
- Price, D.L., Sisodia, S.S., and Gandy, S.E. (1995). Amyloid beta amyloidosis in Alzheimer's disease. *Curr. Opin. Neurol.* 8, 268–274.
- Chen, X.H., Johnson, V.E., Uryu, K., Trojanowski, J.Q., and Smith, D.H. (2009). A lack of amyloid beta plaques despite persistent accumulation of amyloid beta in axons of long-term survivors of traumatic brain injury. *Brain Pathol.* 19, 214–223.
- Chen, X.H., Siman, R., Iwata, A., Meaney, D.F., Trojanowski, J.Q., and Smith, D.H. (2004). Long-term accumulation of amyloid-beta, beta-secretase, presenilin-1, and caspase-3 in damaged axons following brain trauma. *Am. J. Pathol.* 165, 357–371.
- Cirrito, J.R., Yamada, K.A., Finn, M.B., Sloviter, R.S., Bales, K.R., May, P.C., Schoepp, D.D., Paul, S.M., Mennerick, S., and Holtzman, D.M. (2005). Synaptic activity regulates interstitial fluid amyloid-beta levels in vivo. *Neuron* 48, 913–922.
- Loane, D.J., Pocivavsek, A., Moussa, C.E., Thompson, R., Matsuoka, Y., Faden, A.I., Rebeck, G.W., and Burns, M.P. (2009). Amyloid precursor protein secretases as therapeutic targets for traumatic brain injury. *Nat. Med.* 15, 377–379.
- Marklund, N., Blennow, K., Zetterberg, H., Ronne-Engstrom, E., Enblad, P., and Hillered, L. (2009). Monitoring of brain interstitial total tau and beta amyloid proteins by microdialysis in patients with traumatic brain injury. *J. Neurosurg.* 110, 1227–1237.
- Brody, D.L., Magnoni, S., Schwetty, K.E., Spinner, M.L., Esparza, T.J., Stocchetti, N., Zipfel, G.J., and Holtzman, D.M. (2008). Amyloid-beta dynamics correlate with neurological status in the injured human brain. *Science* 321, 1221–1224.
- Graham, D.I., Adams, J.H., and Doyle, D. (1978). Ischaemic brain damage in fatal non-missile head injuries. *J. Neurol. Sci.* 39, 213–234.
- Enblad, P., Frykholm, P., Valtysson, J., Silander, H.C., Andersson, J., Fasth, K.J., Watanabe, Y., Langstrom, B., Hillered, L., and Persson, L. (2001). Middle cerebral artery occlusion and reperfusion in primates monitored by microdialysis and sequential positron emission tomography. *Stroke* 32, 1574–1580.
- Hutchinson, P.J., Gupta, A.K., Fryer, T.F., Al-Rawi, P.G., Chatfield, D.A., Coles, J.P., O'Connell, M.T., Kett-White, R., Minhas, P.S., Aigbirhio, F.I., Clark, J.C., Kirkpatrick, P.J., Menon, D.K., and Pickard, J.D. (2002). Correlation between cerebral blood flow, substrate delivery, and metabolism in head injury: a combined microdialysis and triple oxygen positron emission tomography study. *J. Cereb. Blood Flow Metab.* 22, 735–745.
- Hillered, L., Persson, L., Nilsson, P., Ronne-Engstrom, E., and Enblad, P. (2006). Continuous monitoring of cerebral metabolism in traumatic brain injury: a focus on cerebral microdialysis. *Curr. Opin. Crit. Care* 12, 112–118.
- Hillered, L., Vespa, P.M., and Hovda, D.A. (2005). Translational neurochemical research in acute human brain injury: the current status and potential future for cerebral microdialysis. *J. Neurotrauma* 22, 3–41.
- Bellander, B.M., Cantais, E., Enblad, P., Hutchinson, P., Nordstrom, C.H., Robertson, C., Sahuquillo, J., Smith, M., Stocchetti, N., Ungerstedt, U., Unterberg, A., and Olsen, N.V. (2004). Consensus meeting on microdialysis in neurointensive care. *Intensive Care Med.* 30, 2166–2169.
- Timofeev, I., Carpenter, K.L., Nortje, J., Al-Rawi, P.G., O'Connell, M.T., Czornyka, M., Smielewski, P., Pickard, J.D., Menon, D.K., Kirkpatrick, P.J., Gupta, A.K., and Hutchinson, P.J. (2011). Cerebral extracellular chemistry and outcome following traumatic brain injury: a microdialysis study of 223 patients. *Brain* 134, 484–494.
- Badan, I., Dina, I., Buchhold, B., Suofu, Y., Walker, L., Gratz, M., Platt, D., Kessler, C.H., and Popa-Wagner, A. (2004). Accelerated accumulation of N- and C-terminal beta APP fragments and delayed recovery of microtubule-associated protein 1B expression following stroke in aged rats. *Eur. J. Neurosci.* 19, 2270–2280.

35. Yam, P.S., Takasago, T., Dewar, D., Graham, D.I., and McCulloch, J. (1997). Amyloid precursor protein accumulates in white matter at the margin of a focal ischaemic lesion. *Brain Res.* 760, 150–157.
36. Wen, Y., Onyewuchi, O., Yang, S., Liu, R., and Simpkins, J.W. (2004). Increase in beta-secretase activity and expression in rats following transient cerebral ischemia. *Brain Res.* 1009, 1–8.
37. Koike, M.A., Green, K.N., Blurton-Jones, M., and Laferla, F.M. (2010). Oligemic hypoperfusion differentially affects tau and amyloid- β . *Am. J. Pathol.* 177, 300–310.
38. Wang, X., Xing, A., Xu, C., Cai, Q., Liu, H., and Li, L. (2010). Cerebrovascular hypoperfusion induces spatial memory impairment, synaptic changes, and amyloid- β oligomerization in rats. *J. Alzheimers Dis.* 21, 813–822.
39. Qi, J.P., Wu, H., Yang, Y., Wang, D.D., Chen, Y.X., Gu, Y.H., and Liu, T. (2007). Cerebral ischemia and Alzheimer's disease: the expression of amyloid- β and apolipoprotein E in human hippocampus. *J. Alzheimers Dis.* 12, 335–341.
40. Wisniewski, H.M., and Maslinska, D. (1996). Beta-protein immunoreactivity in the human brain after cardiac arrest. *Folia Neuropathol.* 34, 65–71.
41. Zetterberg, H., Mortberg, E., Song, L., Chang, L., Provuncher, G.K., Patel, P.P., Ferrell, E., Fournier, D.R., Kan, C.W., Campbell, T.G., Meyer, R., Rivnak, A.J., Pink, B.A., Minnehan, K.A., Piech, T., Rissin, D.M., Duffy, D.C., Rubertsson, S., Wilson, D.H., and Blennow, K. (2011). Hypoxia due to cardiac arrest induces a time-dependent increase in serum amyloid beta levels in humans. *PLoS One* 6, e28263.
42. Claeysen, S., Cochet, M., Donneger, R., Dumuis, A., Bockeaert, J., and Giannoni, P. (2012). Alzheimer culprits: cellular crossroads and interplay. *Cell Signal* 24, 1831–1840.
43. Koffie, R.M., Hashimoto, T., Tai, H.C., Kay, K.R., Serrano-Pozo, A., Joyner, D., Hou, S., Kopeikina, K.J., Frosch, M.P., Lee, V.M., Holtzman, D.M., Hyman, B.T., and Spires-Jones, T.L. (2012). Apolipoprotein E4 effects in Alzheimer's disease are mediated by synaptotoxic oligomeric amyloid- β . *Brain* 135, 2155–2168.
44. Texido, L., Hernandez, S., Martín-Satue, M., Povedano, M., Casanovas, A., Esquerda, J., Marsal, J., and Solsona, C. (2011). Sera from amyotrophic lateral sclerosis patients induce the non-canonical activation of NMDA receptors "in vitro". *Neurochem. Int.* 59, 954–964.
45. Magnoni, S., Esparza, T.J., Conte, V., Carbonara, M., Carrabba, G., Holtzman, D.M., Zipfel, G.J., Stocchetti, N., and Brody, D.L. (2012). Tau elevations in the brain extracellular space correlate with reduced amyloid- β levels and predict adverse clinical outcomes after severe traumatic brain injury. *Brain* 135, 1268–1280.
46. Skoglund, K., Enblad, P., and Marklund, N. (2009). Effects of the neurological wake-up test on intracranial pressure and cerebral perfusion pressure in brain-injured patients. *Neurocrit. Care* 11, 135–142.
47. Elf, K., Nilsson, P., and Enblad, P. (2002). Outcome after traumatic brain injury improved by an organized secondary insult program and standardized neurointensive care. *Crit. Care Med.* 30, 2129–2134.
48. Osler, T., Baker, S.P., and Long, W. (1997). A modification of the injury severity score that both improves accuracy and simplifies scoring. *J. Trauma* 43, 922–925.
49. Wilson, J.T., Pettigrew, L.E., and Teasdale, G.M. (1998). Structured interviews for the Glasgow Outcome Scale and the extended Glasgow Outcome Scale: guidelines for their use. *J. Neurotrauma* 15, 573–585.
50. Servadei, F., Murray, G.D., Penny, K., Teasdale, G.M., Dearden, M., Iannotti, F., Lapiere, F., Maas, A.J., Karimi, A., Ohman, J., Persson, L., Stocchetti, N., Trojanowski, T., and Unterberg, A. (2000). The value of the "worst" computed tomographic scan in clinical studies of moderate and severe head injury. *European Brain Injury Consortium. Neurosurgery* 46, 70–75.
51. Marshall, L.F., Marshall, S.B., Klauber, M.R., Van Berkum Clark, M., Eisenberg, H., Jane, J.A., Luerssen, T.G., Marmarou, A., and Foulkes, M.A. (1992). The diagnosis of head injury requires a classification based on computed axial tomography. *J. Neurotrauma* 9, Suppl. 1, S287–292.
52. Ronne-Engstrom, E., Cesarini, K.G., Enblad, P., Hesselager, G., Marklund, N., Nilsson, P., Salci, K., Persson, L., and Hillered, L. (2001). Intracerebral microdialysis in neurointensive care: the use of urea as an endogenous reference compound. *J. Neurosurg.* 94, 397–402.
53. Schulz, M.K., Wang, L.P., Tange, M., and Bjerre, P. (2000). Cerebral microdialysis monitoring: determination of normal and ischemic cerebral metabolisms in patients with aneurysmal subarachnoid hemorrhage. *J. Neurosurg.* 93, 808–814.
54. Reinstrop, P., Stahl, N., Mellergard, P., Uski, T., Ungerstedt, U., and Nordstrom, C.H. (2000). Intracerebral microdialysis in clinical practice: baseline values for chemical markers during wakefulness, anesthesia, and neurosurgery. *Neurosurgery* 47, 701–709.
55. Hansson, O., Zetterberg, H., Vanmechelen, E., Vanderstichele, H., Andreasson, U., Londos, E., Wallin, A., Minthon, L., and Blennow, K. (2010). Evaluation of plasma A β (40) and A β (42) as predictors of conversion to Alzheimer's disease in patients with mild cognitive impairment. *Neurobiol. Aging* 31, 357–367.
56. Roberts, G.W., Gentleman, S.M., Lynch, A., Murray, L., Landon, M., and Graham, D.I. (1994). Beta amyloid protein deposition in the brain after severe head injury: implications for the pathogenesis of Alzheimer's disease. *J. Neurol. Neurosurg. Psychiatry* 57, 419–425.
57. Johnson, V.E., Stewart, W., and Smith, D.H. (2012). Widespread tau and amyloid- β pathology many years after a single traumatic brain injury in humans. *Brain Pathol.* 22, 142–149.
58. Smith, D.H., Chen, X.H., Nonaka, M., Trojanowski, J.Q., Lee, V.M., Saatman, K.E., Leoni, M.J., Xu, B.N., Wolf, J.A., and Meaney, D.F. (1999). Accumulation of amyloid beta and tau and the formation of neurofibrillary inclusions following diffuse brain injury in the pig. *J. Neuropathol. Exp. Neurol.* 58, 982–992.
59. Uryu, K., Chen, X.H., Martinez, D., Browne, K.D., Johnson, V.E., Graham, D.I., Lee, V.M., Trojanowski, J.Q., and Smith, D.H. (2007). Multiple proteins implicated in neurodegenerative diseases accumulate in axons after brain trauma in humans. *Exp. Neurol.* 208, 185–192.
60. Olsson, A., Csajbok, L., Ost, M., Hoglund, K., Nylen, K., Rosengren, L., Nellgard, B., and Blennow, K. (2004). Marked increase of beta-amyloid(1–42) and amyloid precursor protein in ventricular cerebrospinal fluid after severe traumatic brain injury. *J. Neurol.* 251, 870–876.
61. Lagares, A., Ramos, A., Pérez-Núñez, A., Ballenilla, F., Alday, R., Gómez, P.A., Kaen, A., Lobato, R.D. (2009). The role of MR imaging in assessing prognosis after severe and moderate head injury. *Acta Neurochir. (Wien)* 151, 341–356.
62. Haacke, E.M., Duhaime, A.C., Gean, A.D., Riedy, G., Wintermark, M., Mukherjee, P., Brody, D.L., DeGraba, T., Duncan, T.D., Elovic, E., Hurley, R., Latour, L., Smirniotopoulos, J.G., and Smith, D.H. (2010). Common data elements in radiologic imaging of traumatic brain injury. *J. Magn. Reson. Imaging* 32, 516–543.
63. Skandsen, T., Kvistad, K.A., Solheim, O., Strand, I.H., Folvik, M., and Vik, A. (2010). Prevalence and impact of diffuse axonal injury in patients with moderate and severe head injury: a cohort study of early magnetic resonance imaging findings and 1-year outcome. *J. Neurosurg.* 113, 556–563.
64. Rugg-Gunn, F.J., Symms, M.R., Barker, G.J., Greenwood, R., and Duncan, J.S. (2001). Diffusion imaging shows abnormalities after blunt head trauma when conventional magnetic resonance imaging is normal. *J. Neurol. Neurosurg. Psychiatry* 70, 530–533.
65. Arfanakis, K., Haughton, V.M., Carew, J.D., Rogers, B.P., Dempsey, R.J., and Meyerand, M.E. (2002). Diffusion tensor MR imaging in diffuse axonal injury. *Am. J. Neuroradiol.* 23, 794–802.
66. Kinnunen, K.M., Greenwood, R., Powell, J.H., Leech, R., Hawkins, P.C., Bonnelle, V., Patel, M.C., Counsell, S.J., and Sharp, D.J. (2011). White matter damage and cognitive impairment after traumatic brain injury. *Brain* 134, 449–463.
67. Schwetye, K.E., Cirrito, J.R., Esparza, T.J., Mac Donald, C.L., Holtzman, D.M., and Brody, D.L. (2010). Traumatic brain injury reduces soluble extracellular amyloid- β in mice: a methodologically novel combined microdialysis-controlled cortical impact study. *Neurobiol. Dis.* 40, 555–564.
68. Marklund, N., and Hillered, L. (2011). Animal modelling of traumatic brain injury in preclinical drug development: where do we go from here? *Br. J. Pharmacol.* 164, 1207–1229.
69. Kay, A.D., Petzold, A., Kerr, M., Keir, G., Thompson, E., and Nicoll, J.A. (2003). Alterations in cerebrospinal fluid apolipoprotein E and amyloid beta-protein after traumatic brain injury. *J. Neurotrauma* 20, 943–952.
70. Franz, G., Beer, R., Kampfl, A., Engelhardt, K., Schmutzhard, E., Ulmer, H., and Deisenhammer, F. (2003). Amyloid beta 1–42 and tau in cerebrospinal fluid after severe traumatic brain injury. *Neurology* 60, 1457–1461.
71. Raby, C.A., Morganti-Kossmann, M.C., Kossmann, T., Stahel, P.F., Watson, M.D., Evans, L.M., Mehta, P.D., Spiegel, K., Kuo, Y.M.,

- Roher, A.E., and Emmerling, M.R. (1998). Traumatic brain injury increases beta-amyloid peptide 1–42 in cerebrospinal fluid. *J. Neurochem.* 71, 2505–2509.
72. Emmerling, M.R., Morganti-Kossmann, M.C., Kossmann, T., Stahel, P.F., Watson, M.D., Evans, L.M., Mehta, P.D., Spiegel, K., Kuo, Y.M., Roher, A.E., and Raby, C.A. (2000). Traumatic brain injury elevates the Alzheimer's amyloid peptide A beta 42 in human CSF. A possible role for nerve cell injury. *Ann. N. Y. Acad. Sci.* 903, 118–122.
73. Magnoni, S., and Brody, D.L. (2010). New perspectives on amyloid-beta dynamics after acute brain injury: moving between experimental approaches and studies in the human brain. *Arch. Neurol.* 67, 1068–1073.
74. Esparza, T.J., Zhao, H., Cirrito, J.R., Cairns, N.J., Bateman R.J., Holtzman, D.M., and Brody DL. (2013). Amyloid- β oligomerization in Alzheimer dementia versus high-pathology controls. *Ann. Neurol.* 73, 104–119.
75. Lachno, D.R., Emerson, J.K., Vanderstichele, H., Gonzales, C., Martényi, F., Konrad, R.J., Talbot, J.A., Lowe, S.L., Oefinger, P.E., and Dean, R.A. (2012). Validation of a multiplex assay for simultaneous quantification of amyloid- β peptide species in human plasma with utility for measurements in studies of Alzheimer's disease therapeutics. *J. Alzheimers Dis.* 32, 905–918.
76. Johnson-Wood, K., Lee, M., Motter, R., Hu, K., Gordon, G., Barbour, R., Khan, K., Gordon, M., Tan, H., Games, D., Lieberburg, I., Schenk, D., Seubert, P., and McConlogue, L. (1997). Amyloid precursor protein processing and Abeta42 deposition in a transgenic mouse model of Alzheimer disease. *Proc. Natl. Acad. Sci.* 94, 1550–1555.
77. Vanderstichele, H., Van Kerschaver, E., Hesse, C., Davidsson, P., Buyse, M.A., Andreasen, N., Minthon, L., Wallin, A., Blennow, K., and Vanmechelen, E. (2000). Standardization of measurement of beta-amyloid(1–42) in cerebrospinal fluid and plasma. *Amyloid* 7, 245–258.
78. Bibl, M., Esselmann, H., Otto, M., Lewczuk, P., Cepek, L., Rütger, E., Kornhuber, J., and Wiltfang, J. (2004). Cerebrospinal fluid amyloid beta peptide patterns in Alzheimer's disease patients and nondemented controls depend on sample pretreatment: indication of carrier-mediated epitope masking of amyloid beta peptides. *Electrophoresis* 25, 2912–2918.
79. Lachno, D.R., Vanderstichele, H., De Groote, G., Kostanjevecki, V., De Meyer, G., Siemers, E.R., Willey, M.B., Bourdage, J.S., Konrad, R.J., and Dean, R.A. (2009). The influence of matrix type, diurnal rhythm and sample collection and processing on the measurement of plasma beta-amyloid isoforms using the INNO-BIA plasma Abeta forms multiplex assay. *J. Nutr. Health Aging* 13, 220–225.
80. Tanzi, R.E., Moir, R.D., and Wagner, S.L. (2004). Clearance of Alzheimer's Abeta peptide: the many roads to perdition. *Neuron* 43, 605–608.
81. Bjerke, M., Portelius, E., Minthon, L., Wallin, A., Anckarsäter, H., Anckarsäter, R., Andreasen, N., Zetterberg, H., Andreasen, U., and Blennow, K. (2010). Confounding factors influencing amyloid Beta concentration in cerebrospinal fluid. *Int. J. Alzheimers Dis.* 15, 986310.
82. Schipke, C.G., Jessen, F., Teipel, S., Luckhaus, C., Wiltfang, J., Esselmann, H., Frölich, L., Maier, W., Rütger, E., Heppner, F.L., Prokop, S., Heuser, I., and Peters, O. (2011). Long-term stability of Alzheimer's disease biomarker proteins in cerebrospinal fluid. *J. Alzheimers Dis.* 26, 255–262.
83. Cirrito, J.R., Kang, J.E., Lee, J., Stewart, F.R., Verges, D.K., Silverio, L.M., Bu, G., Mennerick, S., and Holtzman, D.M. (2008). Endocytosis is required for synaptic activity-dependent release of amyloid-beta in vivo. *Neuron* 58, 42–51.
84. Kang, J.E., Cirrito, J.R., Dong, H., Csernansky, J.G., and Holtzman, D.M. (2007). Acute stress increases interstitial fluid amyloid-beta via corticotropin-releasing factor and neuronal activity. *Proc. Natl. Acad. Sci.* 104, 10,673–10,678.
85. Kang, J.E., Lim, M.M., Bateman, R.J., Lee, J.J., Smyth, L.P., Cirrito, J.R., Fujiki, N., Nishino, S., and Holtzman, D.M. (2009). Amyloid-beta dynamics are regulated by orexin and the sleep-wake cycle. *Science* 326, 1005–1007.
86. Kamenetz, F., Tomita, T., Hsieh, H., Seabrook, G., Borchelt, D., Iwatsubo, T., Sisodia, S., and Malinow, R. (2003). APP processing and synaptic function. *Neuron* 37, 925–937.
87. Broersen, K., Rousseau, F., and Schymkowitz, J. (2010). The culprit behind amyloid beta peptide related neurotoxicity in Alzheimer's disease: oligomer size or conformation? *Alzheimers Res. Ther.* 2, 12.
88. Hong, S., Quintero-Monzon, O., Ostaszewski, B.L., Podlisy, D.R., Cavanaugh, W.T., Yang, T., Holtzman, D.M., Cirrito, J.R., and Selkoe, D.J. (2011). Dynamic analysis of amyloid beta-protein in behaving mice reveals opposing changes in ISF versus parenchymal Abeta during age-related plaque formation. *J. Neurosci.* 31, 15861–15869.

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